



DCT-SVD Based Hybrid Approach for Digital Watermarking of Medical Images

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Abstract

This study addresses invisible watermarking techniques aimed at preserving patient privacy during the sharing of medical images. Digital watermarking is a significant method for protecting the confidentiality of patient data by securely embedding personal information into medical images. In this study, three different strategies were developed and compared using a DCT-SVD-based hybrid invisible watermarking technique. In the first method, the host image and the watermark were of the same size, and direct embedding was applied. In the second method, the host image was divided into sixteen 128x128 blocks, and the watermark was segmented accordingly and embedded into each block individually. In the third and proposed method, non-diagnostic regions of the image—referred to as dead zones—were automatically detected, and the watermark was embedded only into these areas. This approach preserved the relevant medical data while minimizing image distortion. When the scaling factor was set to 0.01, PSNR values exceeded 40 for most images, and SSIM values were above

0.9. The results demonstrated that the proposed method outperformed the other two in terms of both imperceptibility and robustness.

Keywords: digital watermarking, DCT, SVD, medical images, patient privacy, image processing.

1 Introduction

Digital communication tools, including images, sound, film, and multimedia, have advanced significantly, raising copyright issues that image encryption alone cannot fully resolve. One solution is embedding information within images, a practice known as image watermarking, which helps copyright holders prove ownership without altering the image's appearance. This can be either visible or invisible, with invisible watermarking being more commonly preferred for privacy and security reasons [2]. This study focuses on invisible watermarking.

Watermarking has gained attention in areas like copyright protection, data authenticity, and information embedding. Various methods have been proposed, some focusing on invisibility, others on robustness, or a combination of both [3]. In healthcare, watermarking is crucial for protecting medical images, which are shared across institutions for diagnostic purposes. The challenge is to preserve image quality while maintaining robust watermarking, particularly in regions unrelated to diagnostic content,



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to prevent interference [4]. These issues highlight the need for further advancements in maintaining the authenticity and integrity of medical images [5].

The aim of this study is to embed a hidden message, which includes the patient's radiology report, into specific regions of a medical image. After applying the Discrete Cosine Transform (DCT) to the host image, watermarking is performed by combining the singular values of the host image and watermark image. The goal is to minimize the distortion in the host image while ensuring the robust extraction of the watermark. A literature review of similar research was conducted, considering the characteristics and qualities of medical images. Other digital watermarking algorithms were evaluated to develop a more reliable digital watermarking algorithm for medical images. In this study, a DCT based invisible watermarking technique using Singular Value Decomposition (SVD) was applied, and the ability of the new images to preserve the hidden information was investigated. Then, watermark extraction was performed, and the success of the methods was tested. During the application, 13 medical images were used as hosts, and 2 radiological reports were used as watermarks. The similarity between the original and watermarked images was measured using metrics such as Peak-Signal-to-Noise Ratio (PSNR), Mean Squared Error (MSE), Normalized Correlation (NC), and Structural Similarity Index (SSIM).

2 Related Work

The practice of embedding hidden messages has evolved from Steganography to Cryptology and Digital Watermarking, with numerous studies conducted in this field. In 2004, Alghoniemy et al. [6] developed a watermarking technique that employs geometric shapes in the frequency domain. The robustness of this method was evaluated by introducing white noise at varying levels of intensity to the watermarked image, demonstrating its significant resistance to noise disturbances. In a study by Solachidis and Pitas [1], a circular convolving image watermarking method was introduced. In this method, a circular convolving watermark is added in the frequency domain. The multiplicative addition method was used to keep the watermark visibility ratio low, and correlation was used to test the presence of the watermark in the image. Experimental results showed that the method was resistant to disruptive effects such as JPEG compression, filtering, noise addition, cropping, rotation, and scaling. An algorithm using the Discrete

Wavelet Transform (DWT) method was developed to make the watermarked element resistant to attacks by Elbaşı. In DWT, both the LL and HH bands were used to add PRN, making the watermark resistant to attacks. It was concluded that using both bands in the DWT method resulted in more successful watermarking [3].

In 2009, Aslantas [7] developed an SVD-based image watermarking method, examining the effectiveness of DCT, DFT, and DWT techniques. Various attacks were applied to the watermarked images, and it was observed that the DFT-SVD-based method performed better when the optimal scaling factor was selected. In another study by Aslantaş et al. [8], a DWT-SVD-based image watermarking method was investigated. The watermark scaling factors were optimally determined using the Particle Swarm Optimization (PSO) algorithm, and the proposed technique outperformed methods that used fixed scaling factors.

In the study by Aslantaş and Öz [9], a watermarking technique based on SVD and Differential Evolution Algorithm (DEA) was developed. The watermarked image was obtained by adding the scaled watermark with multiple scaling factors to the singular values of the image. An objective function was defined to evaluate both robustness and visibility, and it was optimized using DEA. As a result, the lowest level of distortion in the image and the highest resistance to attacks were achieved. Furat and Oral [10] examined data storage methods and digital image watermarking algorithms in past studies. These watermarking algorithms were explained in detail, and it was emphasized that these algorithms are generally success-oriented toward specific goals. In the study by Dogan et al. [11], a watermarking application for color images was implemented using the SVD method. In their study, an iris image was embedded in a facial image using the SVD method. During the watermarking process, the watermark was embedded in its original form, regardless of the scaling value used in the SVD-based methods. The results showed that the PSNR values of the images exposed to attacks were higher and more successful compared to similar studies. In the study by Ustubioglu and Ulutas [12], Region of Interest (ROI) and Region of Non-Interest (RONI) areas were used to securely store patient information and maintain the integrity of medical images. Literature studies required small ROI, while the proposed method allowed ROI to be up to 65%. Experimental results showed that the method was effective with high PSNR

and Normalized Correlation (NC) values. In the study by Mamuti and Kazan [5], color images were separated into color channels, and each channel was processed with different watermarking algorithms. The performance of the proposed digital watermarking algorithm was evaluated and analyzed using NC and PSNR. Experimental results showed that the algorithm was successful and effective in achieving acceptable image quality. In the study by Karakiş and Gürkahraman [4], personal patient information and radiology reports in medical images' file headers were encrypted using the AES-256 algorithm. These encrypted data were hidden in pixels in irrelevant areas of the host images, identified using histogram statistics. The watermarking process was performed by combining the singular values obtained from the message and the host image using DWT and SVD methods, and the method was evaluated. The study found that the developed method was imperceptible, resistant to attacks, and had high data hiding capacity compared to similar works in the literature. In the study by Mohammed et al. [2], a hybrid method was used for embedding patient's private information into images by performing DCT and SVD-based image watermarking. PSNR and NC were used for performance evaluation. The results showed that the proposed method was secure and robust. In the study by Priyanka and Maheshkar [13], a new fragile watermarking method based on DCT and trigonometric functions for image authentication was proposed. Grayscale images were divided into 4x4 overlapping blocks, and DCT was applied to each block, with the DC component selected. The selected value was converted into control bits and embedded into the least significant bits of the block as the watermark. Experimental results showed that the method preserved the quality of the watermarked image, made the watermark undetectable, and was successful in detecting regional attacks. In the study by Yıldız et al., watermarking methods used to protect copyright violations and personal data privacy in digital images were examined. A hybrid watermarking technique combining DWT, DCT and SVD was developed, and various types of noise were added to the watermarked images. Optimization algorithms such as Bacterial Foraging Optimization (BFO) and PSO were used to improve the watermark extraction process, which was evaluated using performance metrics like PSNR, Normalized Cross-Correlation (NCC), and Interference Factor (IF). The results showed that the applied techniques were effective, yielding successful outcomes in both watermarking

and watermark extraction processes [14].

3 Methodology

In this study, non-blind invisible watermarking was applied, and reports were embedded into medical images using three different DCT-SVD-based methods, with the watermark being extracted afterward. PSNR, MSE, NC, and SSIM values were compared for different images and reports.

3.1 Images Used

In the experiment phase, a total of 13 medical images were used as host images. These were selected from different imaging modalities: 10 vertebra (MRI), 2 abdomen (ultrasound), and 1 skull radiograph (CR). All images were in DICOM format, grayscale, and had a size of 512x512 pixels. Additionally, two radiology reports were used as watermarks and labeled as W1 and W2. The host images were numbered from I1 to I13. This structure allowed the proposed method to be tested across different anatomical regions and imaging modalities.

3.2 DCT-SVD Based Hybrid Watermarking Methods

In this study, three different methods were compared using a DCT-SVD-based hybrid watermarking technique. In the first method, direct watermarking was applied to a host image that was the same size as the watermark. In the second method, the host image was divided into 16 blocks (4x4), and the watermark was embedded into each block. In the third method, the watermark was embedded only into the non-relevant (non-diagnostic) regions of the host image. The same watermarking technique was used in all methods, with the differences arising from the embedding location and image dimensions.

3.2.1 Method 1: Equal-Sized Host Image and Watermark

Method 1 was implemented by directly embedding the watermark into the entire host image. Both images are grayscale and have a size of 512x512 pixels. The images were preprocessed using `rgb2gray` and `im2double` functions to make them ready for processing. A representative illustration of the host image and the watermark is shown in Figure 1.

The watermarking process begins by applying the DCT to the host image, followed by the application of SVD to the DCT coefficients to obtain the singular values. The same process is applied to the watermark image, and the resulting singular values are added to those

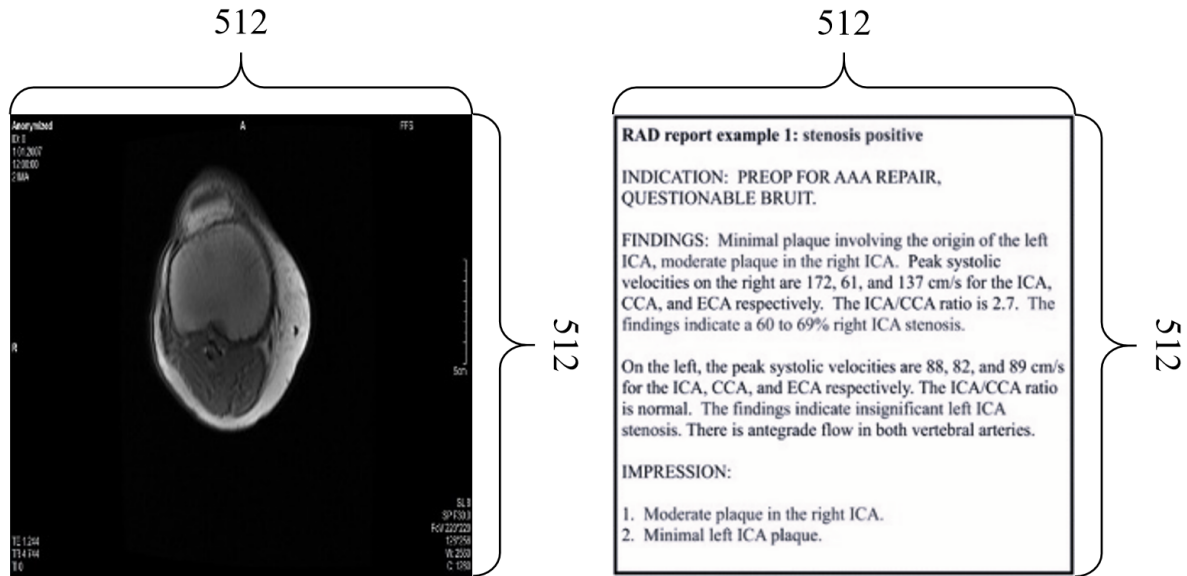


Figure 1. Representative illustration of the host image and the watermark for Method 1.

of the host image using an appropriate scaling factor. The watermarked image is then reconstructed using inverse SVD and inverse DCT.

In the extraction phase, DCT and SVD are applied to the watermarked image, and the singular values of the watermark are retrieved by computing the difference between the singular values of the host and watermarked images. The watermark is then reconstructed accordingly.

3.2.2 Method 2: Block-Based Host Image and Watermark

Method 2 is based on dividing the host image into 16 sub-blocks arranged in a 4×4 grid, each measuring 128×128 pixels. The resized watermark image is embedded separately into each block using the DCT-SVD-based hybrid watermarking method. This approach ensures that the watermark information is evenly distributed across the image, resulting in a more balanced watermarking structure while preserving visual integrity. Additionally, the block-based processing enhances resistance against localized attacks and facilitates the extraction of the watermark. A representative illustration of the host image and the watermark is shown in Figure 2.

During the watermarking process, after obtaining the DCT coefficients of each block, SVD is applied to these coefficients. The singular values of the watermark image are embedded into these SVD components using a predefined scaling factor. The watermark extraction process is performed in a similar manner: DCT followed by SVD is applied to the target block, allowing the watermark information to be successfully

retrieved.

3.2.3 Method 3 (Proposed Approach): Embedding the Segmented Watermark into Non-Informative Regions

Method 3 begins by selecting both the host and watermark images in grayscale format with dimensions of 512×512 pixels. The main objective of this method is to minimize distortion that may occur in medical images during the watermarking process. Based on the previously successful DCT-SVD-based hybrid watermarking approach, this method simultaneously addresses image quality and patient data security.

The novelty of this method lies in its ability to automatically detect "non-informative" or "dead zones" frequently observed in medical images—areas that contain no diagnostic information—and embed the watermark only into these regions. This ensures that diagnostically critical parts of the image remain entirely intact. Thus, patient reports can be securely embedded without damaging meaningful information in the image.

The method is primarily based on arithmetic matrix operations and analyzes transitions between black (non-informative) and white (informative) regions in the grayscale plane. These black regions, often used for patient details such as name or date, are effectively utilized for report watermarking through the proposed algorithm. As a result, patient privacy is preserved, and diagnostic quality is maintained. The steps of the proposed method can be summarized as follows:

- Step 1: The process starts with the preparation

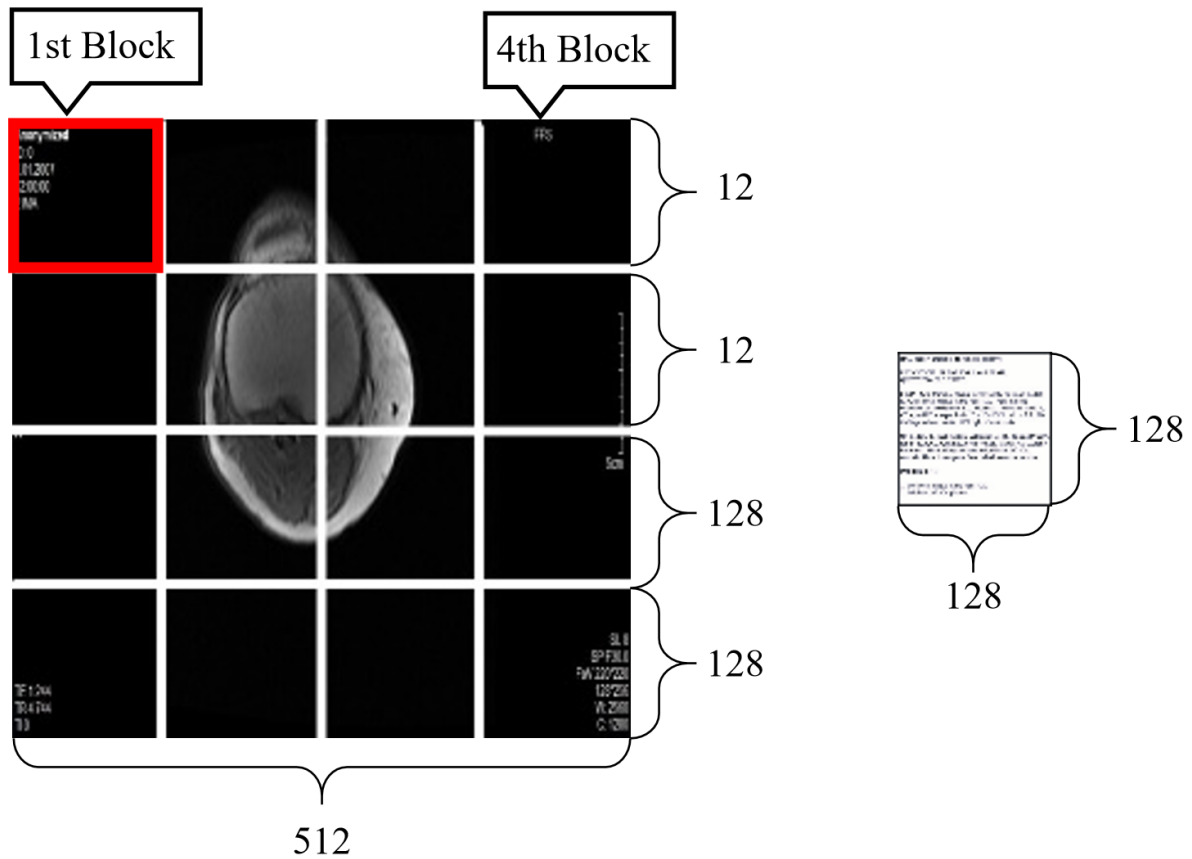


Figure 2. Representative illustration of the host image and the watermark for Method 2.

of the medical image and the watermark report. RGB images are converted to grayscale using the `rgb2gray` function to make them suitable for processing.

- Step 2: A matrix called `matrix_list`, which contains the column-wise pixel sums of the medical image, is generated. This matrix represents the total pixel value for each column.
- Step 3: Threshold values (`val_high` and `val_low`) are determined on a column basis. These values are used to distinguish between informative and non-informative regions and guide where the watermark should be placed.
- Step 4: The patient report image is resized to fit the identified non-informative regions. The `imresize` function is used to align the watermark image with the carrier image dimensions.
- Step 5: The resized report image is prepared so that its central part remains black and is aligned with the medical image. This ensures that informative regions are preserved and the watermark is embedded only into dead zones. At this stage, the image is ready for the watermark embedding and extraction process, just like in

Method 1. In this way, patient data is securely embedded, and diagnostic integrity is preserved.

- Step 6: A two-dimensional DCT is applied to the medical image using the `dct2` function. The resulting DCT coefficients are then processed using SVD to decompose the image into its components.
- Step 7: The new watermark, which has been segmented and resized, is also processed using SVD. This yields the singular values and orthogonal matrices of both images.
- Step 8: The singular values of the watermark are multiplied by an appropriate scaling factor (e.g., 0.01) and added to the singular values of the DCT coefficients of the host image. This allows for invisible watermark integration while maintaining recoverability.
- Step 9: Finally, inverse SVD and inverse DCT operations are performed to obtain the watermarked image. These steps reconstruct the original host image and watermark components. The inverse processes regenerate the image data, resulting in the final watermarked image.

A representative illustration of the host image and the segmented watermark used in the proposed approach (Method 3) is presented in detail in Figure 3. The block diagram of embedding the segmented watermark into the host image using the DCT-SVD-based hybrid watermarking technique is shown in Figure 4. The diagram of the operations performed during the watermark extraction process for Method 3 is shown in Figure 5.

In this study, human intervention was reduced through the automatic detection of dead zones, and the method demonstrated broad applicability and high performance in tests conducted on different types of medical images. The performance was validated using the PSNR, SSIM, MSE, and NC metrics.

Optimization of the Scaling Factor: The scaling factor (SF) is a critical parameter governing the fundamental trade-off between the imperceptibility of the watermarked host image and the robustness of the extracted watermark. To automate and optimize this crucial parameter selection, we can formulate the SF determination as a single-objective optimization problem and employ the Differential Evolution (DE) algorithm to solve it. DE is a population-based evolutionary algorithm renowned for its robustness and efficiency in continuous parameter optimization, making it well-suited for this task.

3.3 Comparison Metrics

Four different evaluation metrics were used to measure the experimental results obtained by the applied methods and to perform a performance comparison.

3.3.1 PSNR

The system calculated the signal-to-noise ratio values between the original image and the watermarked image, as well as between the original watermark and the extracted watermark, according to Equation 1.

$$PSNR = 10 \times \log_{10} \left(\frac{255^2}{\frac{1}{N \times N} \sum_{i=1}^N \sum_{j=1}^N [I_1(i, j) - I_2(i, j)]^2} \right) \quad (1)$$

In the equation:

$10 \times \log_{10}$: This expression is used to calculate the ratio on a logarithmic scale. Multiplying by 10 converts the ratio into decibels (dB).

255 represents the maximum pixel value in an 8-bit image.

N represents the number of pixels along one dimension of the image.

$I_1(i, j)$ represents the pixel value at the i th row and j th column of the original image.

$I_2(i, j)$ represents the pixel value at the i th row and j th column of the reconstructed (watermarked) image.

PSNR is a significant metric used to evaluate the quality of digital images. It measures the similarity between an image and its altered version. Generally, it is used to determine the similarity between the original image and its processed version. A higher PSNR value indicates greater similarity between the images [15–17].

3.3.2 MSE

MSE is a metric used to evaluate how similar two signals are and calculated with Equation 2.

$$MSE = \frac{1}{mn} \sum_{i=0}^{m-1} \sum_{j=0}^{n-1} [I_1(i, j) - I_2(i, j)]^2 \quad (2)$$

In the equation:

$I_1(i, j)$ represents the pixel value at the i -th row and j -th column of the original image.

$I_2(i, j)$ represents the pixel value at the i -th row and j -th column of the reconstructed (watermarked) image.

m and n represent the dimensions of the image.

The MSE value ranges from 0 to ∞ . A higher MSE indicates greater error and, consequently, lower image quality. Conversely, a lower MSE value signifies that the image is closer to the reference image and indicates better image quality [18].

3.3.3 SSIM

SSIM measures the similarity between two images. The SSIM value is derived from a combination of three factors: loss of correlation, luminance distortion, and contrast distortion. This metric reflects the structural similarity between images more effectively [16]. Unlike PSNR, SSIM takes into account luminance and contrast, providing a more accurate perceptual quality assessment. It yields more reliable results than PSNR, especially in cases involving structural distortions. The SSIM metric ranges from $[0, 1]$ and is calculated using Equation 3. If the correlation between two images is low, the SSIM value approaches 0. A value of 1 indicates a high level of correlation. The positive

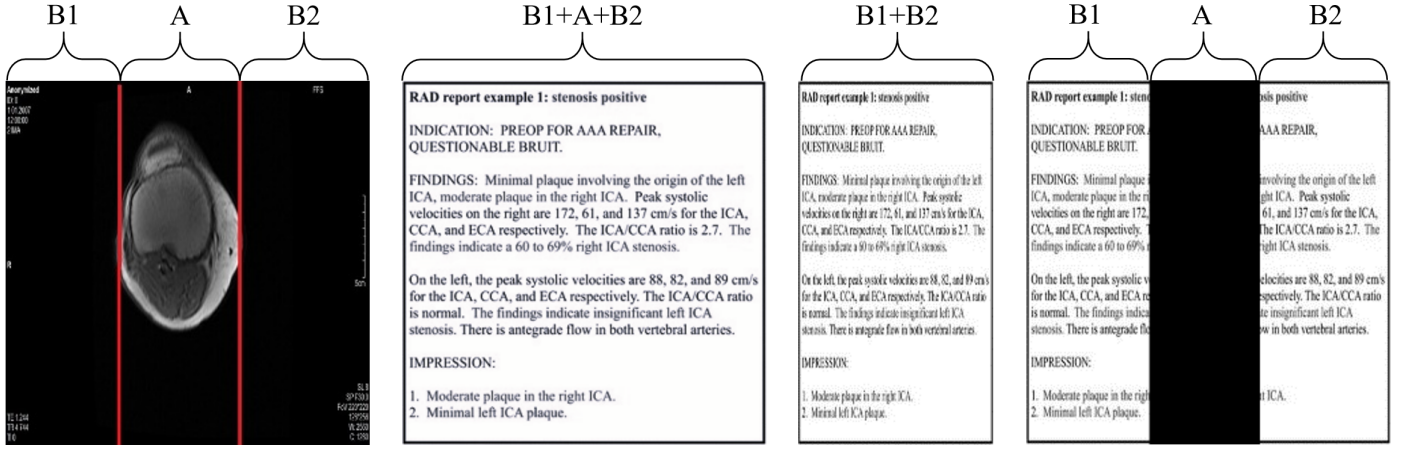


Figure 3. Representative illustration of the host image and the extracted watermark for the proposed method.

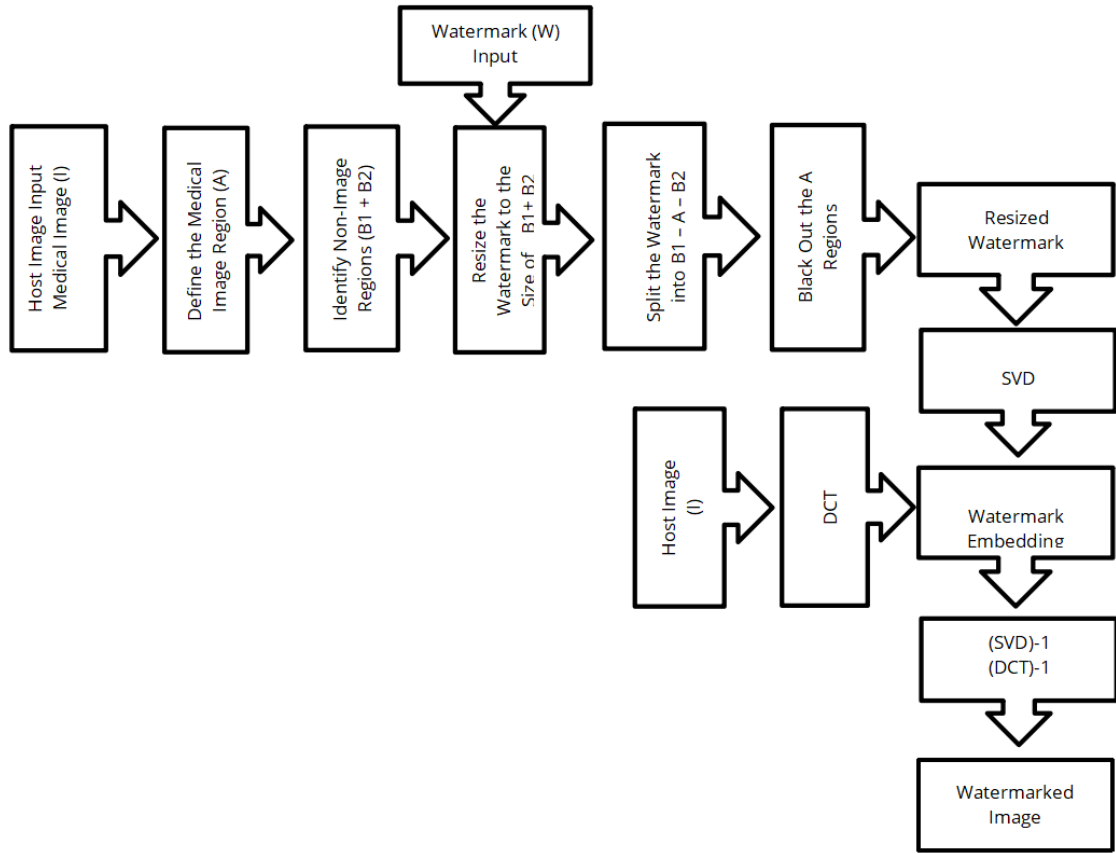


Figure 4. The diagram of the watermark embedding process for the proposed method (Method 3).

constants in Equation 4 (c_1 , c_2 , and c_3) are used to prevent division by zero [16, 18, 19].

$$\text{SSIM}(f, g) = I(f, g)c(f, g)s(f, g) \quad (3)$$

$$I(f, g) = \frac{2\mu_f\mu_g + c_1}{\mu_f^2 + \mu_g^2 + c_1} \quad (4)$$

$$c(f, g) = \frac{2\sigma_f\sigma_g + c_2}{\sigma_f^2 + \sigma_g^2 + c_2} \quad (5)$$

In Equation 4, the $I(f, g)$ is a luminance comparison function that compares the approximate brightness of two images (μ_f and μ_g). This factor reaches the value of 1 only when the two images are identical. The $c(f, g)$ is a contrast comparison function that evaluates the similarity of contrast between two images. Contrast is determined by the standard deviations σ_f and σ_g . When $\sigma_f = \sigma_g$, this term reaches its maximum value of

$$s(f, g) = \frac{\sigma_f\sigma_g + c_3}{\sigma_f\sigma_g + c_3} \quad (6)$$

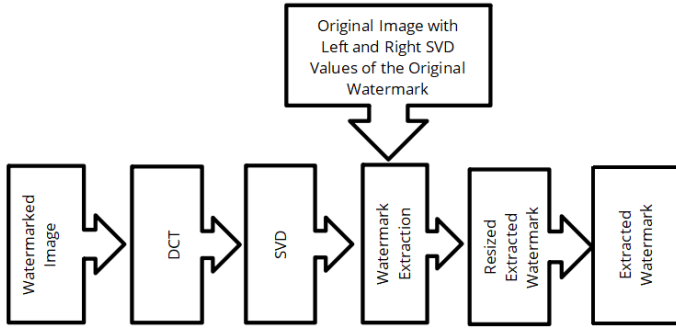


Figure 5. The block diagram of the watermark extraction process for the proposed method.

1. The $s(f, g)$ is a structure comparison function that measures the correlation coefficient between the two images [16, 18, 19].

3.3.4 NC

NC is a quantitative metric used to measure similarity. Therefore, it is used as an indicator of the effectiveness and robustness of watermarking algorithms. NC is calculated according to Equation 5 [2, 5].

$$NC = \frac{\sum_{x=0}^M \sum_{y=0}^N W(x, y) \cdot W'(x, y)}{\sqrt{\sum_{x=0}^M \sum_{y=0}^N W(x, y)^2} \cdot \sqrt{\sum_{x=0}^M \sum_{y=0}^N W'(x, y)^2}} \quad (7)$$

In this equation:

$W(x, y)$ represents the value at coordinates x and y of the original watermark.

$W'(x, y)$ represents the value at coordinates x and y of the extracted watermark.

M denotes the total number of pixels along the horizontal axis of the image.

N denotes the total number of pixels along the vertical axis of the image.

The NC value typically ranges between 0 and 1 when used to measure similarity between two images. This range indicates how similar the two images are. However, in cases of phase shift or negative correlation between images, the NC value can also take negative values. In general, a higher positive NC value indicates greater similarity, while a lower value suggests greater dissimilarity.

4 Experiments

In this study, patient reports were invisibly embedded into medical images using a DCT-SVD-based hybrid watermarking method, and three different strategies

were evaluated. The fundamental processing steps are the same in all methods, with the difference being the location where the watermark is embedded. A non-blind watermarking structure was used, and the results were analyzed using PSNR, SSIM, MSE, and NC metrics, demonstrating that the proposed approach offers high visual quality and robustness.

4.1 Selection and Analysis of the Scaling Factor

In DCT-SVD-based watermarking methods, the selection of the scaling factor (SF) plays a critical role in both the quality of the host image and the robustness of the watermark [11]. As the scaling factor increases, the robustness of the watermark improves; however, this can lead to noticeable distortions in the original image [20]. Conversely, a lower scaling factor preserves the visual integrity of the host image but reduces the robustness of the watermark [14]. Therefore, determining this parameter at an optimal level is essential for the success of the watermarking system [21].

In the scope of this study, experiments were first conducted with different scaling values (ranging from -1 to 1). The obtained findings reveal the similarity between the watermarked and original images (IPSNR and ISSIM) as well as the similarity between the extracted and original watermark (WPSNR and WSSIM). After determining the optimal scaling factor (e.g., 0.01), the three different watermarking methods were evaluated using this fixed value, and the results were compared.

According to the obtained results, the proposed approach, namely the Segmented Watermark method, showed higher PSNR and SSIM values, especially at low scaling factors (0.01–0.05), compared to the other methods. At a scaling factor of 0.01, the IPSNR value was calculated as 44.47 and the ISSIM value as 0.9992. These values indicate high image quality and successful watermark integration. Similarly, the WPSNR and WSSIM metrics also show that the extracted watermark was obtained with high accuracy. The results of Tables 1, 2, 3, 4, 5, 6, 7, 8, 9 and Figure 6 confirm this.

The determination of the scaling factor is generally carried out using trial-and-error and experimental methods. Watermarked images are created using different scaling factors, and the effects of these factors on imperceptibility and confidentiality are examined. In the DCT-SVD-based hybrid watermarking technique, the scaling factor typically ranges between

Table 1. IPSNR, ISSIM, WPSNR and WSSIM values for Method 1 and W1 with different scaling factors.

| SF | Method | Equal-Sized (Method 1) – W1 Block-Based Split Watermark (Proposed Method) | | | | | | | | | | | | |
|------|--------|---|---------------|---------------|---------------|---------------|---------------|---------------|---------------|---------------|---------------|---------------|---------------|---------------|
| | Image | I1 | I2 | I3 | I4 | I5 | I6 | I7 | I8 | I9 | I10 | I11 | I12 | I13 |
| 0.01 | IPSNR | 40.374 | 40.550 | 40.549 | 40.521 | 40.469 | 40.456 | 41.117 | 40.402 | 40.422 | 40.391 | 40.424 | 40.433 | 40.403 |
| | WPSNR | 34.684 | 27.109 | 27.109 | 28.646 | 34.960 | 33.949 | 17.157 | 38.085 | 39.659 | 43.737 | 40.525 | 42.644 | 44.855 |
| | ISSIM | 0.997 | 0.994 | 0.994 | 0.995 | 0.994 | 0.990 | 0.953 | 0.983 | 0.985 | 0.991 | 0.999 | 0.995 | 0.992 |
| | WSSIM | 0.955 | 0.919 | 0.919 | 0.920 | 0.971 | 0.970 | 0.889 | 0.973 | 0.979 | 0.987 | 0.983 | 0.989 | 0.989 |
| 0.03 | IPSNR | 30.899 | 31.101 | 31.101 | 31.075 | 30.999 | 31.008 | 31.670 | 30.899 | 30.910 | 30.901 | 30.949 | 30.899 | 30.899 |
| | WPSNR | 44.003 | 23.881 | 23.878 | 25.072 | 30.252 | 28.654 | 16.649 | 47.118 | 43.584 | 48.308 | 36.480 | 50.939 | 50.073 |
| | ISSIM | 0.989 | 0.956 | 0.956 | 0.960 | 0.957 | 0.942 | 0.826 | 0.927 | 0.933 | 0.945 | 0.992 | 0.965 | 0.951 |
| | WSSIM | 0.991 | 0.878 | 0.878 | 0.883 | 0.954 | 0.950 | 0.875 | 0.994 | 0.989 | 0.996 | 0.983 | 0.997 | 0.996 |
| 0.05 | IPSNR | 26.490 | 26.727 | 26.727 | 26.709 | 26.623 | 26.628 | 27.262 | 26.471 | 26.482 | 26.469 | 26.580 | 26.473 | 26.472 |
| | WPSNR | 26.490 | 22.193 | 22.190 | 23.028 | 26.769 | 25.722 | 16.579 | 45.603 | 41.110 | 47.007 | 30.840 | 48.436 | 48.715 |
| | ISSIM | 0.976 | 0.908 | 0.908 | 0.916 | 0.909 | 0.886 | 0.733 | 0.872 | 0.882 | 0.892 | 0.978 | 0.925 | 0.902 |
| | WSSIM | 0.991 | 0.851 | 0.851 | 0.854 | 0.921 | 0.921 | 0.877 | 0.994 | 0.988 | 0.996 | 0.965 | 0.997 | 0.997 |
| 0.1 | IPSNR | 20.638 | 20.868 | 20.868 | 20.868 | 20.779 | 20.737 | 21.339 | 20.491 | 20.494 | 20.455 | 20.851 | 20.595 | 20.528 |
| | WPSNR | 30.689 | 19.260 | 19.258 | 19.834 | 21.632 | 21.610 | 16.274 | 37.439 | 35.495 | 42.334 | 21.304 | 32.818 | 36.283 |
| | ISSIM | 0.933 | 0.798 | 0.798 | 0.811 | 0.799 | 0.7615 | 0.582 | 0.766 | 0.789 | 0.770 | 0.933 | 0.829 | 0.793 |
| | WSSIM | 0.976 | 0.789 | 0.789 | 0.805 | 0.842 | 0.8587 | 0.877 | 0.987 | 0.977 | 0.994 | 0.881 | 0.984 | 0.990 |
| 0.5 | IPSNR | 12.9505 | 8.933 | 8.933 | 9.136 | 8.824 | 8.439 | 8.868 | 9.226 | 8.423 | 7.211 | 9.804 | 9.049 | 8.624 |
| | WPSNR | 5.328 | 10.009 | 10.009 | 9.643 | 10.252 | 11.348 | 10.011 | 10.880 | 13.223 | 19.508 | 8.533 | 10.682 | 11.912 |
| | ISSIM | 0.640 | 0.357 | 0.357 | 0.367 | 0.359 | 0.329 | 0.240 | 0.365 | 0.381 | 0.360 | 0.607 | 0.422 | 0.390 |
| | WSSIM | 0.638 | 0.515 | 0.515 | 0.518 | 0.525 | 0.569 | 0.533 | 0.818 | 0.827 | 0.891 | 0.575 | 0.703 | 0.731 |
| 0.75 | IPSNR | 12.036 | 6.950 | 6.950 | 7.139 | 6.836 | 6.392 | 6.479 | 7.703 | 7.094 | 4.885 | 8.922 | 7.171 | 6.617 |
| | WPSNR | 3.637 | 7.653 | 7.652 | 7.387 | 7.791 | 8.535 | 7.858 | 7.345 | 8.281 | 13.010 | 5.624 | 7.803 | 8.688 |
| | ISSIM | 0.572 | 0.271 | 0.271 | 0.276 | 0.269 | 0.243 | 0.172 | 0.286 | 0.302 | 0.289 | 0.518 | 0.340 | 0.321 |
| | WSSIM | 0.482 | 0.486 | 0.486 | 0.486 | 0.484 | 0.502 | 0.429 | 0.716 | 0.737 | 0.751 | 0.487 | 0.616 | 0.629 |

Table 2. IPSNR, ISSIM, WPSNR and WSSIM values for Method 1 and W2 with different scaling factors

| SF | Method | Equal-Sized (Method 1) – W2 Block-Based Split Watermark (Proposed Method) | | | | | | | | | | | | |
|------|--------|---|---------------|---------------|---------------|---------------|---------------|---------------|---------------|---------------|---------------|---------------|---------------|---------------|
| | Image | I1 | I2 | I3 | I4 | I5 | I6 | I7 | I8 | I9 | I10 | I11 | I12 | I13 |
| 0.01 | IPSNR | 40.760 | 40.922 | 40.922 | 40.863 | 40.838 | 40.823 | 41.457 | 40.767 | 40.764 | 40.732 | 40.750 | 40.788 | 40.776 |
| | WPSNR | 38.270 | 26.940 | 26.942 | 28.789 | 35.087 | 33.498 | 17.547 | 37.225 | 39.409 | 42.367 | 40.245 | 43.434 | 42.435 |
| | ISSIM | 0.999 | 0.995 | 0.995 | 0.996 | 0.996 | 0.993 | 0.960 | 0.988 | 0.989 | 0.993 | 0.999 | 0.997 | 0.994 |
| | WSSIM | 0.980 | 0.926 | 0.926 | 0.931 | 0.980 | 0.968 | 0.909 | 0.978 | 0.980 | 0.990 | 0.985 | 0.993 | 0.990 |
| 0.03 | IPSNR | 31.258 | 31.478 | 31.478 | 31.443 | 31.366 | 31.380 | 32.029 | 31.254 | 31.265 | 31.252 | 31.310 | 31.253 | 31.253 |
| | WPSNR | 46.160 | 23.678 | 23.676 | 24.956 | 29.943 | 28.148 | 16.914 | 45.577 | 42.591 | 46.688 | 35.999 | 50.154 | 49.218 |
| | ISSIM | 0.994 | 0.962 | 0.962 | 0.967 | 0.964 | 0.951 | 0.843 | 0.942 | 0.946 | 0.955 | 0.995 | 0.972 | 0.960 |
| | WSSIM | 0.996 | 0.884 | 0.884 | 0.896 | 0.900 | 0.944 | 0.889 | 0.995 | 0.991 | 0.996 | 0.986 | 0.997 | 0.997 |
| 0.05 | IPSNR | 26.840 | 27.115 | 27.115 | 27.087 | 26.995 | 27.006 | 27.626 | 26.826 | 26.838 | 26.825 | 26.825 | 26.825 | 26.823 |
| | WPSNR | 43.293 | 21.943 | 21.942 | 22.892 | 26.535 | 25.236 | 16.807 | 43.450 | 40.049 | 45.782 | 30.120 | 47.803 | 47.966 |
| | ISSIM | 0.987 | 0.920 | 0.920 | 0.929 | 0.921 | 0.899 | 0.754 | 0.881 | 0.900 | 0.908 | 0.985 | 0.939 | 0.918 |
| | WSSIM | 0.995 | 0.859 | 0.859 | 0.871 | 0.934 | 0.913 | 0.887 | 0.996 | 0.990 | 0.996 | 0.970 | 0.997 | 0.997 |
| 0.1 | IPSNR | 20.967 | 21.276 | 21.276 | 21.263 | 21.172 | 21.137 | 21.711 | 20.850 | 20.855 | 20.811 | 21.266 | 20.953 | 20.889 |
| | WPSNR | 31.936 | 18.939 | 18.938 | 19.651 | 21.400 | 21.144 | 16.424 | 36.068 | 34.363 | 40.845 | 20.780 | 32.948 | 35.609 |
| | ISSIM | 0.958 | 0.816 | 0.816 | 0.830 | 0.818 | 0.780 | 0.602 | 0.788 | 0.809 | 0.792 | 0.949 | 0.848 | 0.816 |
| | WSSIM | 0.984 | 0.803 | 0.803 | 0.821 | 0.865 | 0.855 | 0.879 | 0.989 | 0.984 | 0.993 | 0.902 | 0.988 | 0.990 |
| 0.5 | IPSNR | 13.092 | 9.308 | 9.307 | 9.513 | 9.234 | 8.859 | 9.337 | 9.436 | 8.650 | 7.594 | 10.131 | 9.406 | 8.998 |
| | WPSNR | 5.873 | 10.037 | 10.036 | 9.732 | 10.224 | 11.203 | 9.965 | 11.597 | 13.948 | 19.061 | 8.723 | 10.816 | 11.919 |
| | ISSIM | 0.702 | 0.374 | 0.374 | 0.385 | 0.376 | 0.344 | 0.247 | 0.372 | 0.391 | 0.372 | 0.649 | 0.440 | 0.409 |
| | WSSIM | 0.609 | 0.466 | 0.465 | 0.460 | 0.479 | 0.518 | 0.507 | 0.821 | 0.832 | 0.865 | 0.540 | 0.661 | 0.683 |
| 0.75 | IPSNR | 12.245 | 7.259 | 7.259 | 7.463 | 7.148 | 6.709 | 6.934 | 7.909 | 7.261 | 5.197 | 8.942 | 7.399 | 6.876 |
| | WPSNR | 4.086 | 7.868 | 7.868 | 7.606 | 7.981 | 8.670 | 7.896 | 7.897 | 8.907 | 13.059 | 6.135 | 8.172 | 8.989 |
| | ISSIM | 0.630 | 0.281 | 0.281 | 0.287 | 0.279 | 0.252 | 0.177 | 0.289 | 0.305 | 0.298 | 0.545 | 0.348 | 0.332 |
| | WSSIM | 0.436 | 0.418 | 0.418 | 0.412 | 0.418 | 0.429 | 0.374 | 0.697 | 0.725 | 0.683 | 0.425 | 0.553 | 0.563 |

-1 and 1 [7].

The PSNR and SSIM values between the original images and the watermarked images, as well as between the original watermarks and the extracted

watermarks for different scaling factors, are presented in the tables for the medical images and watermarks used. The graphical representation of the PSNR values, obtained by selecting the I1 medical image and the W1

Table 3. IPSNR, ISSIM, WPSNR and WSSIM values for Method 2 and W1 with different scaling factors.

| SF | Method | Block-Based (Method 2) – W1 | | | | | | | | | | | | |
|------|--------|-----------------------------|---------------|---------------|---------------|---------------|---------------|---------------|---------------|---------------|---------------|---------------|---------------|---------------|
| | Image | I1 | I2 | I3 | I4 | I5 | I6 | I7 | I8 | I9 | I10 | I11 | I12 | I13 |
| 0.01 | IPSNR | 40.459 | 40.561 | 40.561 | 40.548 | 40.519 | 40.581 | 42.051 | 40.519 | 40.493 | 40.466 | 40.740 | 40.765 | 40.788 |
| | WPSNR | 15.628 | 14.801 | 14.809 | 14.799 | 14.804 | 14.826 | 14.644 | 16.598 | 17.126 | 14.822 | 14.795 | 14.873 | 14.869 |
| | ISSIM | 0.994 | 0.987 | 0.987 | 0.987 | 0.987 | 0.988 | 0.982 | 0.983 | 0.989 | 0.990 | 0.995 | 0.994 | 0.994 |
| | WSSIM | 0.715 | 0.725 | 0.724 | 0.724 | 0.724 | 0.724 | 0.722 | 0.656 | 0.589 | 0.725 | 0.724 | 0.724 | 0.724 |
| 0.03 | IPSNR | 31.250 | 31.234 | 31.234 | 31.201 | 31.168 | 31.255 | 32.625 | 31.138 | 31.117 | 30.962 | 31.514 | 31.554 | 31.555 |
| | WPSNR | 15.906 | 15.110 | 15.112 | 15.107 | 15.108 | 15.155 | 14.817 | 16.863 | 17.038 | 15.163 | 15.186 | 15.217 | 15.214 |
| | ISSIM | 0.972 | 0.950 | 0.950 | 0.950 | 0.950 | 0.950 | 0.929 | 0.933 | 0.955 | 0.957 | 0.982 | 0.977 | 0.976 |
| | WSSIM | 0.712 | 0.725 | 0.726 | 0.725 | 0.725 | 0.725 | 0.724 | 0.651 | 0.576 | 0.724 | 0.725 | 0.724 | 0.725 |
| 0.05 | IPSNR | 26.972 | 26.971 | 26.971 | 26.930 | 26.889 | 27.020 | 28.226 | 26.782 | 26.765 | 26.542 | 27.335 | 27.361 | 27.360 |
| | WPSNR | 16.079 | 15.386 | 15.393 | 15.387 | 15.401 | 15.461 | 15.026 | 16.993 | 16.952 | 15.435 | 15.471 | 15.539 | 15.485 |
| | ISSIM | 0.948 | 0.916 | 0.916 | 0.917 | 0.917 | 0.914 | 0.885 | 0.885 | 0.917 | 0.922 | 0.971 | 0.958 | 0.956 |
| | WSSIM | 0.710 | 0.724 | 0.724 | 0.723 | 0.724 | 0.722 | 0.724 | 0.646 | 0.563 | 0.723 | 0.723 | 0.723 | 0.725 |
| 0.1 | IPSNR | 21.250 | 21.371 | 21.371 | 21.305 | 21.268 | 21.440 | 22.444 | 20.945 | 20.891 | 20.594 | 21.901 | 21.793 | 21.799 |
| | WPSNR | 16.424 | 16.135 | 16.149 | 16.136 | 16.144 | 16.205 | 15.415 | 17.214 | 16.714 | 16.143 | 16.248 | 16.287 | 16.268 |
| | ISSIM | 0.889 | 0.843 | 0.843 | 0.844 | 0.844 | 0.836 | 0.801 | 0.786 | 0.835 | 0.839 | 0.941 | 0.910 | 0.905 |
| | WSSIM | 0.706 | 0.718 | 0.718 | 0.718 | 0.717 | 0.716 | 0.723 | 0.640 | 0.541 | 0.718 | 0.714 | 0.714 | 0.715 |
| 0.5 | IPSNR | 12.182 | 9.527 | 9.527 | 9.480 | 9.527 | 9.509 | 10.755 | 9.188 | 8.785 | 8.284 | 10.749 | 10.129 | 10.082 |
| | WPSNR | 17.352 | 16.728 | 16.719 | 16.750 | 16.766 | 16.744 | 17.637 | 16.698 | 16.291 | 16.759 | 16.735 | 16.682 | 16.635 |
| | ISSIM | 0.607 | 0.508 | 0.508 | 0.511 | 0.512 | 0.494 | 0.480 | 0.404 | 0.432 | 0.486 | 0.690 | 0.597 | 0.585 |
| | WSSIM | 0.609 | 0.544 | 0.543 | 0.546 | 0.548 | 0.546 | 0.649 | 0.542 | 0.512 | 0.548 | 0.543 | 0.537 | 0.534 |
| 0.75 | IPSNR | 10.817 | 7.280 | 7.280 | 7.280 | 7.299 | 7.248 | 8.485 | 7.379 | 7.084 | 6.054 | 8.833 | 7.810 | 7.777 |
| | WPSNR | 16.673 | 16.401 | 16.384 | 16.398 | 16.395 | 16.460 | 17.126 | 16.411 | 16.291 | 16.393 | 16.403 | 16.300 | 16.291 |
| | ISSIM | 0.558 | 0.408 | 0.409 | 0.409 | 0.412 | 0.396 | 0.383 | 0.314 | 0.327 | 0.410 | 0.579 | 0.495 | 0.490 |
| | WSSIM | 0.540 | 0.519 | 0.518 | 0.520 | 0.520 | 0.522 | 0.575 | 0.525 | 0.512 | 0.519 | 0.519 | 0.513 | 0.512 |

Table 4. IPSNR, ISSIM, WPSNR and WSSIM values for Method 2 and W2 with different scaling factors.

| SF | Method | Block-Based (Method 2) – W2 | | | | | | | | | | | | |
|------|--------|-----------------------------|---------------|---------------|---------------|---------------|---------------|---------------|---------------|---------------|---------------|---------------|---------------|---------------|
| | Image | I1 | I2 | I3 | I4 | I5 | I6 | I7 | I8 | I9 | I10 | I11 | I12 | I13 |
| 0.01 | IPSNR | 40.907 | 40.949 | 40.950 | 40.941 | 40.911 | 40.977 | 42.462 | 40.910 | 40.866 | 40.848 | 41.156 | 41.155 | 41.171 |
| | WPSNR | 14.961 | 13.717 | 13.719 | 13.732 | 13.766 | 13.781 | 13.763 | 15.454 | 14.008 | 13.808 | 13.812 | 13.874 | 13.861 |
| | ISSIM | 0.995 | 0.989 | 0.989 | 0.989 | 0.989 | 0.990 | 0.986 | 0.986 | 0.992 | 0.992 | 0.995 | 0.995 | 0.995 |
| | WSSIM | 0.513 | 0.544 | 0.544 | 0.545 | 0.544 | 0.544 | 0.537 | 0.390 | 0.322 | 0.547 | 0.543 | 0.544 | 0.545 |
| 0.03 | IPSNR | 31.629 | 31.644 | 31.644 | 31.610 | 31.576 | 31.660 | 33.042 | 31.522 | 31.501 | 31.357 | 31.915 | 31.939 | 31.938 |
| | WPSNR | 15.146 | 14.018 | 14.027 | 14.029 | 14.063 | 14.061 | 13.996 | 15.468 | 13.864 | 14.095 | 14.088 | 14.133 | 14.132 |
| | ISSIM | 0.978 | 0.956 | 0.956 | 0.956 | 0.956 | 0.955 | 0.938 | 0.941 | 0.963 | 0.962 | 0.983 | 0.979 | 0.978 |
| | WSSIM | 0.505 | 0.540 | 0.540 | 0.540 | 0.539 | 0.539 | 0.539 | 0.386 | 0.316 | 0.539 | 0.540 | 0.540 | 0.539 |
| 0.05 | IPSNR | 27.340 | 27.386 | 27.386 | 27.344 | 27.299 | 27.428 | 28.646 | 27.163 | 27.149 | 26.944 | 27.725 | 27.746 | 27.747 |
| | WPSNR | 15.301 | 14.221 | 14.231 | 14.220 | 14.248 | 14.269 | 14.183 | 15.414 | 13.727 | 14.262 | 27.725 | 14.334 | 14.326 |
| | ISSIM | 0.955 | 0.923 | 0.923 | 0.923 | 0.923 | 0.921 | 0.896 | 0.895 | 0.926 | 0.930 | 0.971 | 0.960 | 0.959 |
| | WSSIM | 0.493 | 0.536 | 0.536 | 0.534 | 0.535 | 0.532 | 0.539 | 0.382 | 0.311 | 0.534 | 0.532 | 0.530 | 0.532 |
| 0.1 | IPSNR | 21.619 | 21.807 | 21.807 | 21.740 | 21.694 | 21.866 | 22.858 | 21.320 | 21.277 | 21.000 | 22.319 | 22.194 | 22.200 |
| | WPSNR | 15.469 | 14.576 | 14.578 | 14.566 | 14.623 | 14.673 | 14.475 | 15.227 | 13.226 | 14.653 | 14.718 | 14.780 | 14.773 |
| | ISSIM | 0.900 | 0.851 | 0.851 | 0.851 | 0.851 | 0.844 | 0.814 | 0.796 | 0.844 | 0.850 | 0.940 | 0.912 | 0.908 |
| | WSSIM | 0.477 | 0.507 | 0.507 | 0.508 | 0.507 | 0.505 | 0.536 | 0.377 | 0.296 | 0.511 | 0.502 | 0.499 | 0.502 |
| 0.5 | IPSNR | 12.416 | 9.938 | 9.938 | 9.895 | 9.935 | 9.930 | 11.261 | 9.510 | 9.114 | 8.648 | 11.221 | 10.566 | 10.516 |
| | WPSNR | 14.555 | 12.440 | 12.426 | 12.459 | 12.485 | 12.223 | 14.751 | 13.061 | 12.042 | 12.394 | 12.113 | 12.086 | 12.092 |
| | ISSIM | 0.619 | 0.512 | 0.512 | 0.516 | 0.515 | 0.497 | 0.487 | 0.400 | 0.423 | 0.486 | 0.685 | 0.593 | 0.579 |
| | WSSIM | 0.360 | 0.277 | 0.276 | 0.278 | 0.281 | 0.265 | 0.372 | 0.285 | 0.245 | 0.277 | 0.252 | 0.251 | 0.250 |
| 0.75 | IPSNR | 11.052 | 7.628 | 7.628 | 7.628 | 7.662 | 7.635 | 8.958 | 7.629 | 7.315 | 6.433 | 9.154 | 8.196 | 8.168 |
| | WPSNR | 12.968 | 12.105 | 12.092 | 12.162 | 12.189 | 12.055 | 13.756 | 12.467 | 12.042 | 12.139 | 12.042 | 12.042 | 12.042 |
| | ISSIM | 0.567 | 0.406 | 0.406 | 0.408 | 0.410 | 0.393 | 0.385 | 0.306 | 0.317 | 0.402 | 0.577 | 0.488 | 0.480 |
| | WSSIM | 0.282 | 0.249 | 0.248 | 0.253 | 0.255 | 0.246 | 0.319 | 0.265 | 0.245 | 0.252 | 0.245 | 0.245 | 0.245 |

watermark, is provided in Figure 7. When the other results are examined, it is observed that changes in the scaling factor do not affect the performance ranking of the methods across different images, nor does the

choice of image alter this ranking.

To analyze Figure 7 in detail, the PSNR variations for each scaling factor are examined. The graph

Table 5. IPSNR, ISSIM, WPSNR and WSSIM values for Method 3 and W1 with different scaling factors.

| SF | Method | Segmented Watermark (Method 3) – W1 | | | | | | | | | | | | |
|------|--------|-------------------------------------|---------------|---------------|---------------|---------------|---------------|---------------|---------------|---------------|---------------|---------------|---------------|---------------|
| | Image | I1 | I2 | I3 | I4 | I5 | I6 | I7 | I8 | I9 | I10 | I11 | I12 | I13 |
| 0.01 | IPSNR | 44.465 | 42.706 | 42.705 | 42.747 | 42.698 | 42.905 | 43.921 | 42.532 | 43.295 | 44.097 | 42.797 | 42.470 | 42.549 |
| | WPSNR | 27.932 | 28.745 | 28.757 | 30.269 | 37.053 | 36.319 | 17.505 | 36.405 | 39.494 | 38.812 | 38.404 | 40.786 | 41.842 |
| | ISSIM | 0.999 | 0.997 | 0.997 | 0.997 | 0.997 | 0.995 | 0.970 | 0.989 | 0.990 | 0.996 | 0.999 | 0.998 | 0.995 |
| | WSSIM | 0.969 | 0.915 | 0.914 | 0.919 | 0.969 | 0.974 | 0.889 | 0.965 | 0.976 | 0.970 | 0.980 | 0.985 | 0.986 |
| 0.03 | IPSNR | 34.678 | 33.304 | 33.304 | 33.342 | 33.279 | 33.497 | 34.529 | 33.029 | 33.834 | 34.664 | 33.259 | 33.012 | 33.040 |
| | WPSNR | 43.925 | 24.963 | 24.964 | 26.224 | 32.218 | 30.607 | 16.782 | 47.779 | 46.218 | 47.932 | 38.813 | 51.761 | 50.871 |
| | ISSIM | 0.994 | 0.970 | 0.970 | 0.973 | 0.971 | 0.962 | 0.875 | 0.945 | 0.954 | 0.971 | 0.995 | 0.975 | 0.965 |
| | WSSIM | 0.993 | 0.878 | 0.878 | 0.892 | 0.966 | 0.962 | 0.868 | 0.995 | 0.994 | 0.996 | 0.989 | 0.997 | 0.997 |
| 0.05 | IPSNR | 30.246 | 28.921 | 28.921 | 28.955 | 28.891 | 29.104 | 30.120 | 28.594 | 29.408 | 30.239 | 28.859 | 28.582 | 28.608 |
| | WPSNR | 45.451 | 23.313 | 23.314 | 24.367 | 28.894 | 27.795 | 16.687 | 47.541 | 43.994 | 49.840 | 34.541 | 51.503 | 51.029 |
| | ISSIM | 0.988 | 0.935 | 0.934 | 0.942 | 0.936 | 0.920 | 0.794 | 0.899 | 0.916 | 0.937 | 0.986 | 0.947 | 0.927 |
| | WSSIM | 0.995 | 0.851 | 0.851 | 0.866 | 0.943 | 0.940 | 0.869 | 0.996 | 0.993 | 0.998 | 0.981 | 0.998 | 0.998 |
| 0.1 | IPSNR | 24.270 | 23.014 | 23.014 | 23.061 | 22.991 | 23.177 | 24.155 | 22.594 | 23.404 | 24.225 | 23.015 | 22.614 | 22.610 |
| | WPSNR | 40.954 | 20.763 | 20.761 | 21.441 | 23.949 | 23.743 | 16.585 | 41.298 | 39.364 | 47.696 | 25.121 | 40.255 | 44.012 |
| | ISSIM | 0.962 | 0.844 | 0.844 | 0.857 | 0.847 | 0.818 | 0.653 | 0.808 | 0.839 | 0.851 | 0.955 | 0.868 | 0.836 |
| | WSSIM | 0.994 | 0.805 | 0.805 | 0.819 | 0.879 | 0.886 | 0.872 | 0.993 | 0.988 | 0.997 | 0.925 | 0.994 | 0.996 |
| 0.5 | IPSNR | 14.110 | 10.422 | 10.422 | 10.633 | 10.395 | 10.272 | 11.082 | 10.393 | 10.262 | 10.307 | 11.199 | 10.454 | 10.148 |
| | WPSNR | 8.456 | 11.742 | 11.742 | 11.448 | 12.152 | 13.651 | 12.178 | 13.930 | 18.781 | 32.642 | 10.269 | 12.732 | 14.174 |
| | ISSIM | 0.720 | 0.428 | 0.428 | 0.441 | 0.434 | 0.404 | 0.306 | 0.425 | 0.475 | 0.462 | 0.678 | 0.484 | 0.447 |
| | WSSIM | 0.777 | 0.499 | 0.499 | 0.506 | 0.522 | 0.602 | 0.624 | 0.865 | 0.876 | 0.974 | 0.584 | 0.739 | 0.781 |
| 0.75 | IPSNR | 13.013 | 8.135 | 8.135 | 8.368 | 8.040 | 7.739 | 8.328 | 8.563 | 7.361 | 9.273 | 8.197 | 7.719 | 13.013 |
| | WPSNR | 5.520 | 9.261 | 9.261 | 8.955 | 9.548 | 10.780 | 9.863 | 9.322 | 20.995 | 7.660 | 9.589 | 10.772 | 5.520 |
| | ISSIM | 0.641 | 0.318 | 0.318 | 0.328 | 0.320 | 0.297 | 0.223 | 0.331 | 0.365 | 0.562 | 0.380 | 0.356 | 0.641 |
| | WSSIM | 0.639 | 0.478 | 0.478 | 0.479 | 0.480 | 0.519 | 0.473 | 0.781 | 0.905 | 0.520 | 0.651 | 0.679 | 0.639 |

Table 6. IPSNR, ISSIM, WPSNR and WSSIM values for Method 3 and W2 with different scaling factors.

| SF | Method | Segmented Watermark (Method 3) – W2 | | | | | | | | | | | | |
|------|--------|-------------------------------------|---------------|---------------|---------------|---------------|---------------|---------------|---------------|---------------|---------------|---------------|---------------|---------------|
| | Image | I1 | I2 | I3 | I4 | I5 | I6 | I7 | I8 | I9 | I10 | I11 | I12 | I13 |
| 0.01 | IPSNR | 44.432 | 42.689 | 42.690 | 42.731 | 42.682 | 42.892 | 43.905 | 42.863 | 43.626 | 44.429 | 43.146 | 42.822 | 42.864 |
| | WPSNR | 28.189 | 28.764 | 28.760 | 30.363 | 37.218 | 36.295 | 17.514 | 34.977 | 36.571 | 36.754 | 38.680 | 39.302 | 41.519 |
| | ISSIM | 0.999 | 0.996 | 0.996 | 0.997 | 0.997 | 0.995 | 0.970 | 0.992 | 0.992 | 0.998 | 0.999 | 0.998 | 0.997 |
| | WSSIM | 0.967 | 0.911 | 0.911 | 0.923 | 0.967 | 0.974 | 0.891 | 0.967 | 0.973 | 0.976 | 0.987 | 0.985 | 0.987 |
| 0.03 | IPSNR | 35.018 | 33.687 | 33.687 | 33.715 | 33.647 | 33.872 | 34.892 | 33.382 | 34.192 | 35.031 | 33.622 | 33.365 | 33.391 |
| | WPSNR | 43.704 | 24.645 | 24.644 | 26.071 | 31.865 | 30.032 | 17.048 | 47.446 | 44.691 | 47.165 | 38.434 | 50.898 | 50.424 |
| | ISSIM | 0.997 | 0.975 | 0.975 | 0.978 | 0.976 | 0.968 | 0.891 | 0.957 | 0.965 | 0.978 | 0.997 | 0.980 | 0.973 |
| | WSSIM | 0.994 | 0.901 | 0.902 | 0.915 | 0.972 | 0.961 | 0.900 | 0.996 | 0.994 | 0.997 | 0.990 | 0.998 | 0.997 |
| 0.05 | IPSNR | 30.601 | 29.309 | 29.309 | 29.336 | 29.266 | 29.480 | 30.486 | 28.949 | 29.764 | 30.593 | 29.228 | 28.936 | 28.962 |
| | WPSNR | 29.336 | 29.266 | 29.480 | 30.486 | 28.949 | 29.764 | 30.593 | 29.228 | 28.936 | 28.962 | 29.336 | 29.266 | 29.480 |
| | ISSIM | 0.994 | 0.944 | 0.944 | 0.951 | 0.946 | 0.931 | 0.813 | 0.917 | 0.932 | 0.949 | 0.991 | 0.957 | 0.941 |
| | WSSIM | 0.998 | 0.877 | 0.877 | 0.889 | 0.954 | 0.938 | 0.898 | 0.997 | 0.993 | 0.997 | 0.983 | 0.998 | 0.998 |
| 0.1 | IPSNR | 24.619 | 23.420 | 23.420 | 23.456 | 23.379 | 23.572 | 24.523 | 22.954 | 23.764 | 24.581 | 23.419 | 22.971 | 22.968 |
| | WPSNR | 41.825 | 20.375 | 20.374 | 21.201 | 23.663 | 23.158 | 16.771 | 39.192 | 37.864 | 46.261 | 24.225 | 40.264 | 43.247 |
| | ISSIM | 0.981 | 0.861 | 0.861 | 0.874 | 0.864 | 0.836 | 0.675 | 0.830 | 0.859 | 0.872 | 0.967 | 0.885 | 0.858 |
| | WSSIM | 0.996 | 0.831 | 0.831 | 0.844 | 0.903 | 0.887 | 0.891 | 0.994 | 0.990 | 0.997 | 0.937 | 0.995 | 0.996 |
| 0.5 | IPSNR | 14.286 | 10.853 | 10.853 | 11.056 | 10.849 | 10.718 | 11.542 | 10.632 | 10.589 | 10.675 | 11.646 | 10.873 | 10.551 |
| | WPSNR | 9.142 | 11.560 | 11.560 | 11.382 | 11.945 | 13.334 | 12.039 | 14.742 | 19.101 | 30.424 | 10.196 | 12.684 | 14.019 |
| | ISSIM | 0.782 | 0.449 | 0.449 | 0.464 | 0.454 | 0.422 | 0.315 | 0.440 | 0.493 | 0.480 | 0.719 | 0.507 | 0.471 |
| | WSSIM | 0.780 | 0.476 | 0.476 | 0.468 | 0.505 | 0.578 | 0.618 | 0.881 | 0.890 | 0.964 | 0.583 | 0.723 | 0.754 |
| 0.75 | IPSNR | 13.162 | 8.480 | 8.483 | 8.732 | 8.428 | 8.138 | 8.816 | 8.765 | 7.751 | 9.494 | 8.501 | 8.051 | 13.162 |
| | WPSNR | 6.072 | 9.361 | 9.361 | 9.082 | 9.575 | 10.690 | 9.772 | 9.976 | 20.363 | 8.005 | 9.841 | 10.917 | 6.072 |
| | ISSIM | 0.708 | 0.334 | 0.334 | 0.345 | 0.337 | 0.312 | 0.231 | 0.341 | 0.379 | 0.604 | 0.398 | 0.373 | 0.708 |
| | WSSIM | 0.618 | 0.422 | 0.422 | 0.415 | 0.428 | 0.462 | 0.449 | 0.774 | 0.886 | 0.475 | 0.601 | 0.626 | 0.618 |

compares the PSNR values of three different methods (Equal-Sized, Block-Based, and Segmented Watermark (Method 3)) on the I1 image. For a scaling factor of 0.01:

- PSNR_I (Equal-Sized): 40.374
- PSNR_W (Equal-Sized): 34.684
- PSNR_I (Block-Based): 40.460

Table 7. Results obtained for both watermarks using a 0.01 scaling factor according to Method 1.

| Image | W1 | | | | | | | | W2 | | | | | | | |
|-------|--------|--------|----------|----------|--------|--------|-------|-------|---------|--------|----------|----------|--------|--------|-------|-------|
| | PSNR_I | PSNR_W | MSE_I | MSE_W | SSIM_I | SSIM_W | NC_I | NC_W | PSNR_I | PSNR_W | MSE_I | MSE_W | SSIM_I | SSIM_W | NC_I | NC_W |
| I1 | 40.374 | 34.684 | 9.174e-5 | 3.400e-4 | 0.997 | 0.955 | 0.999 | 0.994 | 40.760 | 38.270 | 8.393e-5 | 1.489e-4 | 0.999 | 0.980 | 0.999 | 0.998 |
| I2 | 40.550 | 27.109 | 8.810e-5 | 1.945e-4 | 0.994 | 0.919 | 0.999 | 0.983 | 40.922 | 26.940 | 8.086e-5 | 2.023e-3 | 0.995 | 0.926 | 0.999 | 0.991 |
| I3 | 40.549 | 27.109 | 8.810e-5 | 1.945e-4 | 0.994 | 0.919 | 0.999 | 0.983 | 40.922 | 26.942 | 8.086e-5 | 2.021e-3 | 0.995 | 0.926 | 0.999 | 0.991 |
| I4 | 40.521 | 28.646 | 8.868e-5 | 1.365e-3 | 0.995 | 0.920 | 0.999 | 0.987 | 40.863 | 28.789 | 8.196e-5 | 1.321e-3 | 0.996 | 0.931 | 0.999 | 0.993 |
| I5 | 40.469 | 34.960 | 8.976e-5 | 3.191e-4 | 0.994 | 0.971 | 0.999 | 0.997 | 40.838 | 35.087 | 8.244e-5 | 3.099e-4 | 0.996 | 0.980 | 0.999 | 0.998 |
| I6 | 40.456 | 33.949 | 9.001e-5 | 4.027e-4 | 0.990 | 0.970 | 0.999 | 0.997 | 40.823 | 33.498 | 8.272e-5 | 4.468e-4 | 0.993 | 0.968 | 0.999 | 0.998 |
| I7 | 41.117 | 17.157 | 7.730e-5 | 1.924e-2 | 0.953 | 0.889 | 0.999 | 0.979 | 41.457 | 17.547 | 7.149e-5 | 1.759e-2 | 0.960 | 0.909 | 0.999 | 0.991 |
| I8 | 40.402 | 38.085 | 9.113e-5 | 1.554e-4 | 0.983 | 0.973 | 0.999 | 0.997 | 40.767 | 37.225 | 8.380e-5 | 1.894e-4 | 0.988 | 0.978 | 0.999 | 0.998 |
| I9 | 40.422 | 39.659 | 9.072e-5 | 1.081e-4 | 0.985 | 0.979 | 0.999 | 0.998 | 40.764 | 39.409 | 8.385e-5 | 1.145e-4 | 0.989 | 0.980 | 0.999 | 0.999 |
| I10 | 40.391 | 43.737 | 9.137e-5 | 4.229e-5 | 0.991 | 0.987 | 0.999 | 0.999 | 40.732 | 42.367 | 8.447e-5 | 5.797e-5 | 0.993 | 0.990 | 0.999 | 0.999 |
| I11 | 40.424 | 40.525 | 9.068e-5 | 8.861e-5 | 0.999 | 0.983 | 0.999 | 0.998 | 40.750 | 40.245 | 8.413e-5 | 9.451e-5 | 0.999 | 0.985 | 0.999 | 0.999 |
| I12 | 40.433 | 42.644 | 9.049e-5 | 5.439e-5 | 0.995 | 0.989 | 0.999 | 0.999 | 40.7884 | 43.434 | 8.339e-5 | 4.534e-5 | 0.997 | 0.993 | 0.999 | 0.999 |
| I13 | 40.403 | 44.855 | 9.112e-5 | 3.269e-5 | 0.992 | 0.989 | 0.999 | 0.999 | 40.7762 | 42.435 | 8.363e-5 | 5.707e-5 | 0.994 | 0.990 | 0.999 | 0.999 |

Table 8. Results obtained for both watermarks using a 0.01 scaling factor according to Method 2.

| Image | W1 | | | | | | | | W2 | | | | | | | |
|-------|--------|--------|----------|--------|--------|--------|-------|-------|--------|--------|----------|--------|--------|--------|-------|-------|
| | PSNR_I | PSNR_W | MSE_I | MSE_W | SSIM_I | SSIM_W | NC_I | NC_W | PSNR_I | PSNR_W | MSE_I | MSE_W | SSIM_I | SSIM_W | NC_I | NC_W |
| I1 | 40.459 | 15.628 | 8.995e-5 | 17.696 | 0.994 | 0.715 | 0.999 | 0.802 | 40.907 | 14.961 | 8.113e-5 | 24.427 | 0.995 | 0.513 | 0.999 | 0.804 |
| I2 | 40.561 | 14.801 | 8.787e-5 | 20.886 | 0.987 | 0.725 | 0.999 | 0.810 | 40.949 | 13.717 | 8.035e-5 | 30.404 | 0.989 | 0.544 | 0.999 | 0.780 |
| I3 | 40.561 | 14.809 | 8.787e-5 | 20.840 | 0.987 | 0.724 | 0.999 | 0.810 | 40.950 | 13.719 | 8.035e-5 | 30.373 | 0.989 | 0.544 | 0.999 | 0.780 |
| I4 | 40.548 | 14.799 | 8.814e-5 | 20.824 | 0.987 | 0.724 | 0.999 | 0.809 | 40.941 | 13.732 | 8.050e-5 | 30.311 | 0.989 | 0.545 | 0.999 | 0.780 |
| I5 | 40.519 | 14.804 | 8.872e-5 | 20.855 | 0.987 | 0.724 | 0.999 | 0.810 | 40.911 | 13.766 | 8.106e-5 | 30.233 | 0.989 | 0.544 | 0.999 | 0.782 |
| I6 | 40.581 | 14.826 | 8.747e-5 | 20.762 | 0.988 | 0.724 | 0.999 | 0.809 | 40.977 | 13.781 | 7.985e-5 | 30.279 | 0.990 | 0.544 | 0.999 | 0.783 |
| I7 | 42.051 | 14.644 | 6.235e-5 | 21.805 | 0.982 | 0.722 | 0.999 | 0.819 | 42.462 | 13.763 | 5.672e-5 | 32.614 | 0.986 | 0.537 | 0.999 | 0.805 |
| I8 | 40.519 | 16.598 | 8.873e-5 | 11.828 | 0.983 | 0.656 | 0.999 | 0.720 | 40.910 | 15.454 | 8.108e-5 | 15.295 | 0.986 | 0.390 | 0.999 | 0.769 |
| I9 | 40.493 | 17.126 | 8.926e-5 | 4.2023 | 0.989 | 0.589 | 0.999 | 0.523 | 40.866 | 14.008 | 8.191e-5 | 7.300 | 0.992 | 0.322 | 0.999 | 0.613 |
| I10 | 40.466 | 14.822 | 8.982e-5 | 20.855 | 0.990 | 0.725 | 0.999 | 0.812 | 40.848 | 13.808 | 8.225e-5 | 30.388 | 0.992 | 0.547 | 0.999 | 0.786 |
| I11 | 40.740 | 14.795 | 8.433e-5 | 20.980 | 0.995 | 0.724 | 0.999 | 0.812 | 41.156 | 13.812 | 7.662e-5 | 30.357 | 0.995 | 0.543 | 0.999 | 0.786 |
| I12 | 40.765 | 14.873 | 8.384e-5 | 20.653 | 0.994 | 0.724 | 0.999 | 0.811 | 41.155 | 13.874 | 7.664e-5 | 30.139 | 0.995 | 0.544 | 0.999 | 0.788 |
| I13 | 40.788 | 14.869 | 8.339e-5 | 20.684 | 0.994 | 0.724 | 0.999 | 0.811 | 41.171 | 13.861 | 7.636e-5 | 30.062 | 0.995 | 0.545 | 0.999 | 0.787 |

Table 9. Results obtained for both watermarks using a 0.01 scaling factor according to Method 3.

| Image | W1 | | | | | | | | W2 | | | | | | | |
|-------|--------|--------|----------|----------|--------|--------|-------|-------|--------|--------|----------|----------|--------|--------|-------|-------|
| | PSNR_I | PSNR_W | MSE_I | MSE_W | SSIM_I | SSIM_W | NC_I | NC_W | PSNR_I | PSNR_W | MSE_I | MSE_W | SSIM_I | SSIM_W | NC_I | NC_W |
| I1 | 44.465 | 27.932 | 3.576e-5 | 1.609e-3 | 0.999 | 0.969 | 0.999 | 0.996 | 44.432 | 28.189 | 3.603e-5 | 1.517e-3 | 0.999 | 0.967 | 1 | 0.998 |
| I2 | 42.706 | 28.745 | 5.362e-5 | 1.334e-3 | 0.997 | 0.915 | 0.999 | 0.984 | 42.689 | 28.764 | 5.382e-5 | 1.329e-3 | 0.996 | 0.911 | 0.999 | 0.992 |
| I3 | 42.705 | 28.757 | 5.363e-5 | 1.331e-3 | 0.997 | 0.914 | 0.999 | 0.984 | 42.690 | 28.760 | 5.382e-5 | 1.330e-3 | 0.996 | 0.911 | 0.999 | 0.992 |
| I4 | 42.747 | 30.269 | 5.311e-5 | 9.399e-4 | 0.997 | 0.919 | 0.999 | 0.987 | 42.731 | 30.363 | 5.331e-5 | 9.196e-4 | 0.997 | 0.923 | 0.999 | 0.995 |
| I5 | 42.698 | 37.053 | 5.372e-5 | 1.970e-4 | 0.997 | 0.969 | 0.999 | 0.996 | 42.682 | 37.218 | 5.391e-5 | 1.897e-4 | 0.997 | 0.967 | 0.999 | 0.998 |
| I6 | 42.905 | 36.319 | 5.121e-5 | 2.333e-4 | 0.995 | 0.974 | 0.999 | 0.997 | 42.892 | 36.295 | 5.137e-5 | 2.346e-4 | 0.995 | 0.974 | 0.999 | 0.998 |
| I7 | 43.921 | 17.505 | 4.053e-5 | 1.776e-2 | 0.970 | 0.889 | 0.999 | 0.977 | 43.905 | 17.514 | 4.069e-5 | 1.772e-2 | 0.970 | 0.891 | 0.999 | 0.988 |
| I8 | 42.532 | 36.405 | 5.581e-5 | 2.287e-4 | 0.989 | 0.965 | 0.999 | 0.996 | 42.863 | 34.977 | 5.172e-5 | 3.178e-4 | 0.992 | 0.967 | 0.999 | 0.997 |
| I9 | 43.295 | 39.494 | 4.682e-5 | 1.123e-4 | 0.990 | 0.976 | 0.999 | 0.998 | 43.626 | 36.571 | 4.338e-5 | 2.202e-4 | 0.992 | 0.973 | 0.999 | 0.998 |
| I10 | 44.097 | 38.812 | 3.893e-5 | 1.314e-4 | 0.996 | 0.970 | 0.999 | 0.997 | 44.429 | 36.754 | 3.606e-5 | 2.111e-4 | 0.998 | 0.976 | 0.999 | 0.998 |
| I11 | 42.797 | 38.404 | 5.251e-5 | 1.443e-4 | 0.999 | 0.980 | 0.999 | 0.998 | 43.146 | 38.680 | 4.846e-5 | 1.355e-4 | 0.999 | 0.987 | 0.999 | 0.999 |
| I12 | 42.470 | 40.786 | 5.661e-5 | 8.343e-5 | 0.998 | 0.985 | 0.999 | 0.998 | 42.822 | 39.302 | 5.220e-5 | 1.174e-4 | 0.998 | 0.985 | 0.999 | 0.999 |
| I13 | 42.549 | 41.842 | 5.560e-5 | 6.542e-5 | 0.995 | 0.986 | 0.999 | 0.999 | 42.864 | 41.519 | 5.170e-5 | 7.048e-5 | 0.997 | 0.987 | 0.999 | 0.999 |

- PSNR_W (Block-Based): 15.629
- PSNR_I (Segmented Watermark (Method 3)): 44.466
- PSNR_W (Segmented Watermark (Method 3)): 27.932

The Segmented Watermark (Method 3) achieves higher values in both PSNR_I and PSNR_W metrics compared to the other methods, indicating high image quality and high watermark quality. For a scaling factor of 0.03:

- PSNR_I (Equal-Sized): 30.899
- PSNR_W (Equal-Sized): 44.003
- PSNR_I (Block-Based): 31.251
- PSNR_W (Block-Based): 15.907

- PSNR_I (Segmented Watermark (Method 3)): 34.679
- PSNR_W (Segmented Watermark (Method 3)): 43.926

The Segmented Watermark (Method 3) again demonstrates superiority in both PSNR_I and PSNR_W, with PSNR_I significantly higher than the other methods. For a scaling factor of 0.05:

- PSNR_I (Equal-Sized): 26.491
- PSNR_W (Equal-Sized): 26.491
- PSNR_I (Block-Based): 26.973
- PSNR_W (Block-Based): 16.079
- PSNR_I (Segmented Watermark (Method 3)): 30.247

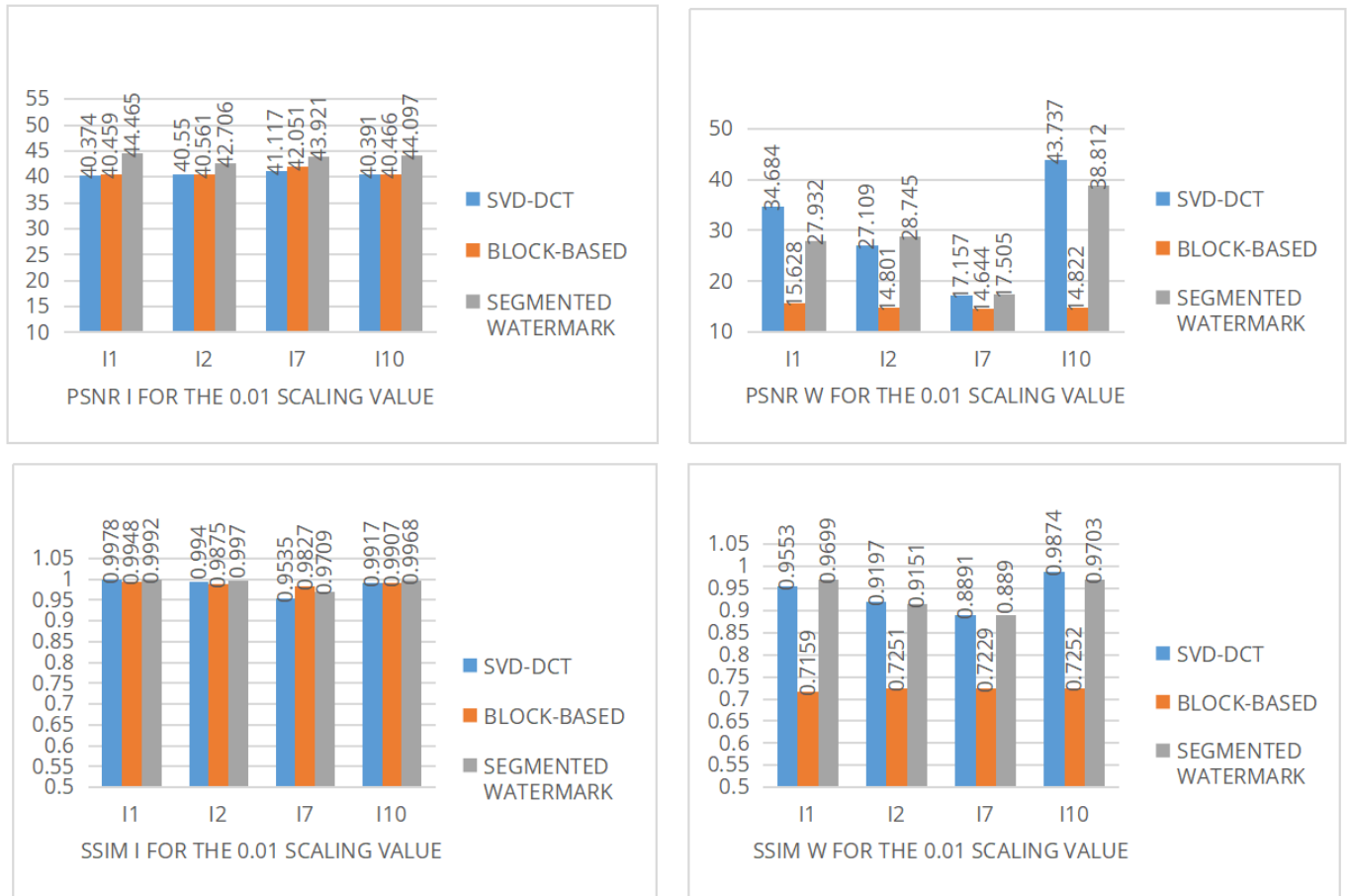


Figure 6. Graph of the variations in IPSNR, ISSIM, WPSNR and WSSIM for images I1, I2, I7, and I10 using a 0.01 scaling factor.

- PSNR_W (Segmented Watermark (Method 3)): 45.451

The Segmented Watermark (Method 3) performs particularly well in PSNR_W and also achieves higher PSNR_I than the other methods. For a scaling factor of 0.1:

- PSNR_I (Equal-Sized): 20.639
- PSNR_W (Equal-Sized): 30.690
- PSNR_I (Block-Based): 21.251
- PSNR_W (Block-Based): 16.425
- PSNR_I (Segmented Watermark (Method 3)): 24.271
- PSNR_W (Segmented Watermark (Method 3)): 40.954

Again, the Segmented Watermark (Method 3) yields higher PSNR_I and PSNR_W values than the other methods. For a scaling factor of 0.5:

- PSNR_I (Equal-Sized): 12.951

- PSNR_W (Equal-Sized): 5.329
- PSNR_I (Block-Based): 12.182
- PSNR_W (Block-Based): 17.353
- PSNR_I (Segmented Watermark (Method 3)): 14.111
- PSNR_W (Segmented Watermark (Method 3)): 8.457

Although the Block-Based method shows higher PSNR_W, the Segmented Watermark (Method 3) provides a more balanced performance with higher PSNR_I overall. For a scaling factor of 0.75:

- PSNR_I (Equal-Sized): 12.037
- PSNR_W (Equal-Sized): 3.637
- PSNR_I (Block-Based): 10.818
- PSNR_W (Block-Based): 16.673
- PSNR_I (Segmented Watermark (Method 3)): 13.013

- PSNR_W (Segmented Watermark (Method 3)): 5.520

Again, the Block-Based method achieves higher PSNR_W, but the Segmented Watermark (Method 3) performs better in PSNR_I.

Overall, analyzing Figure 7, it can be concluded that the Segmented Watermark (Method 3) outperforms the other methods in both image quality (PSNR_I) and extracted watermark quality (PSNR_W). Especially at low scaling factors (0.01, 0.03, 0.05), the Segmented Watermark (Method 3) demonstrates significantly better performance. As the scaling factor increases (0.5 and 0.75), the difference with other methods decreases, but the Segmented Watermark (Method 3) still maintains high PSNR_I values.

The graphical representation of the SSIM values, obtained by selecting the I1 medical image and the W1 watermark, is provided in Figure 8. Examining the SSIM variations for each scaling factor, the graph compares three different methods (Equal-Sized, Block-Based, and Segmented Watermark (Method 3)) on the I1 image. For a scaling factor of 0.01:

- SSIM_I (Equal-Sized): 0.99782
- SSIM_W (Equal-Sized): 0.95539
- SSIM_I (Block-Based): 0.99489
- SSIM_W (Block-Based): 0.71593
- SSIM_I (Segmented Watermark (Method 3)): 0.99922
- SSIM_W (Segmented Watermark (Method 3)): 0.96998

The Segmented Watermark (Method 3) achieves higher values in both SSIM_I and SSIM_W, indicating high image similarity and high watermark quality. For a scaling factor of 0.03:

- SSIM_I (Equal-Sized): 0.98784
- SSIM_W (Equal-Sized): 0.99144
- SSIM_I (Block-Based): 0.97290
- SSIM_W (Block-Based): 0.71729
- SSIM_I (Segmented Watermark (Method 3)): 0.99436
- SSIM_W (Segmented Watermark (Method 3)): 0.99378

The Segmented Watermark (Method 3) again demonstrates superiority, especially in SSIM_W. For a scaling factor of 0.05:

- SSIM_I (Equal-Sized): 0.97668
- SSIM_W (Equal-Sized): 0.99149
- SSIM_I (Block-Based): 0.94884
- SSIM_W (Block-Based): 0.71012
- SSIM_I (Segmented Watermark (Method 3)): 0.98842
- SSIM_W (Segmented Watermark (Method 3)): 0.99597

The Segmented Watermark (Method 3) achieves very high SSIM_W and also superior SSIM_I values. For a scaling factor of 0.1:

- SSIM_I (Equal-Sized): 0.93397
- SSIM_W (Equal-Sized): 0.97662
- SSIM_I (Block-Based): 0.88909
- SSIM_W (Block-Based): 0.70614
- SSIM_I (Segmented Watermark (Method 3)): 0.96274
- SSIM_W (Segmented Watermark (Method 3)): 0.99490

Again, the Segmented Watermark (Method 3) shows higher SSIM_I and SSIM_W than the other methods. For a scaling factor of 0.5:

- SSIM_I (Equal-Sized): 0.64047
- SSIM_W (Equal-Sized): 0.63839
- SSIM_I (Block-Based): 0.60779
- SSIM_W (Block-Based): 0.60925
- SSIM_I (Segmented Watermark (Method 3)): 0.72036
- SSIM_W (Segmented Watermark (Method 3)): 0.77700

Although the Equal-Sized method shows higher SSIM_W, the Segmented Watermark (Method 3) provides a more balanced performance and higher SSIM_I overall. For a scaling factor of 0.75:

- SSIM_I (Equal-Sized): 0.57220
- SSIM_W (Equal-Sized): 0.48215
- SSIM_I (Block-Based): 0.55811

- SSIM_W (Block-Based): 0.54041
- SSIM_I (Segmented Watermark (Method 3)): 0.64186
- SSIM_W (Segmented Watermark (Method 3)): 0.63976

The Block-Based method achieves higher SSIM_W, but the Segmented Watermark (Method 3) performs better in SSIM_I. Considering Tables 1, 2, 3, 4, 5, 6, 7, 8, 9 and Figures 6, 7, 8 to determine the optimal scaling range, it is clear that the most suitable range is between 0.01 and 0.05, where high image quality and watermark quality are balanced. More specifically:

- Scaling factor 0.01: Highest image quality with good watermark quality
- Scaling factor 0.03: Balanced and high quality
- Scaling factor 0.05: High watermark quality with acceptable image quality

Therefore, 0.01 and 0.03 appear particularly optimal, as in this range, image and watermark quality are most effectively balanced. As the scaling factor increases, especially beyond 0.1, a noticeable decrease in image quality is observed, indicating that values above 0.1 are not suitable for watermarking. Thus, the ideal range for watermarking operations can be considered between 0.01 and 0.05, with 0.01 being the most optimal value within this range.

As a result of the analysis, it was determined that the scaling factor range between 0.01 and 0.05 is the most suitable. Within this range, an ideal balance between image quality and watermark quality can be achieved. When the scaling factor is selected as 0.01, it was observed that the proposed method provides both high-quality host images and robust watermark extraction.

4.2 Analysis of the Results of Compared Methods

In line with the conducted analyses, when different scaling factors were examined, significant quality degradation was observed in both the host image and the extracted watermark, especially for values of 0.1 and above. Therefore, the range between 0.01 and 0.05 was evaluated as the most suitable interval in terms of both image and watermark quality. In particular, the 0.01 scaling factor stood out as the ideal value, minimizing image distortion while preserving watermark extractability.

Method 1 is based on using the host and watermark

images in the same size. In this method, the quality of the original image remains high, and the visual similarity yields quite successful results. However, the quality of the extracted watermark is not always consistent.

Method 2 presents a block-based approach in which the host image is divided into smaller regions for processing. In this structure, distortion in the host image is quite low; however, the quality of the watermark is significantly reduced. In many cases, the extracted watermarks show low similarity.

The proposed Method 3 is based on embedding the watermark into the non-informative regions of the medical images. Thanks to this strategy, the essential parts of the host image are preserved, and high quality is achieved in both the host and watermark images. In terms of visual similarity (SSIM) and distortion measurements (PSNR, MSE), Method 3 has shown consistent and superior performance compared to the other two methods.

Overall, Method 3 stands out as the most appropriate approach for secure and invisible watermarking in medical images by providing the best balance between image and watermark quality. Especially in scenarios where patient privacy is critical, this method is recommended.

The superiority of the proposed Method 3 can be attributed to its selective embedding strategy. By targeting non-informative regions of medical images, the method avoids altering diagnostically significant pixels. This selective embedding minimizes pixel-level differences between the original and watermarked images, leading to higher PSNR values. Moreover, structural similarities are preserved in informative regions, resulting in higher SSIM values. Unlike Method 1 and Method 2, where watermark embedding may interfere with critical regions or be diluted across blocks, Method 3 ensures that the watermark is robustly embedded without compromising image quality. Consequently, both the host image and the extracted watermark maintain high fidelity, demonstrating the effectiveness of segmenting non-informative regions for watermark embedding.

4.3 Discussion and Conclusion

To evaluate the robustness of the proposed Method 3, various types of attacks were applied and the resulting watermark quality metrics were analyzed. Common digital attacks such as rotation, salt-and-pepper noise, JPEG compression, and sharpening were considered

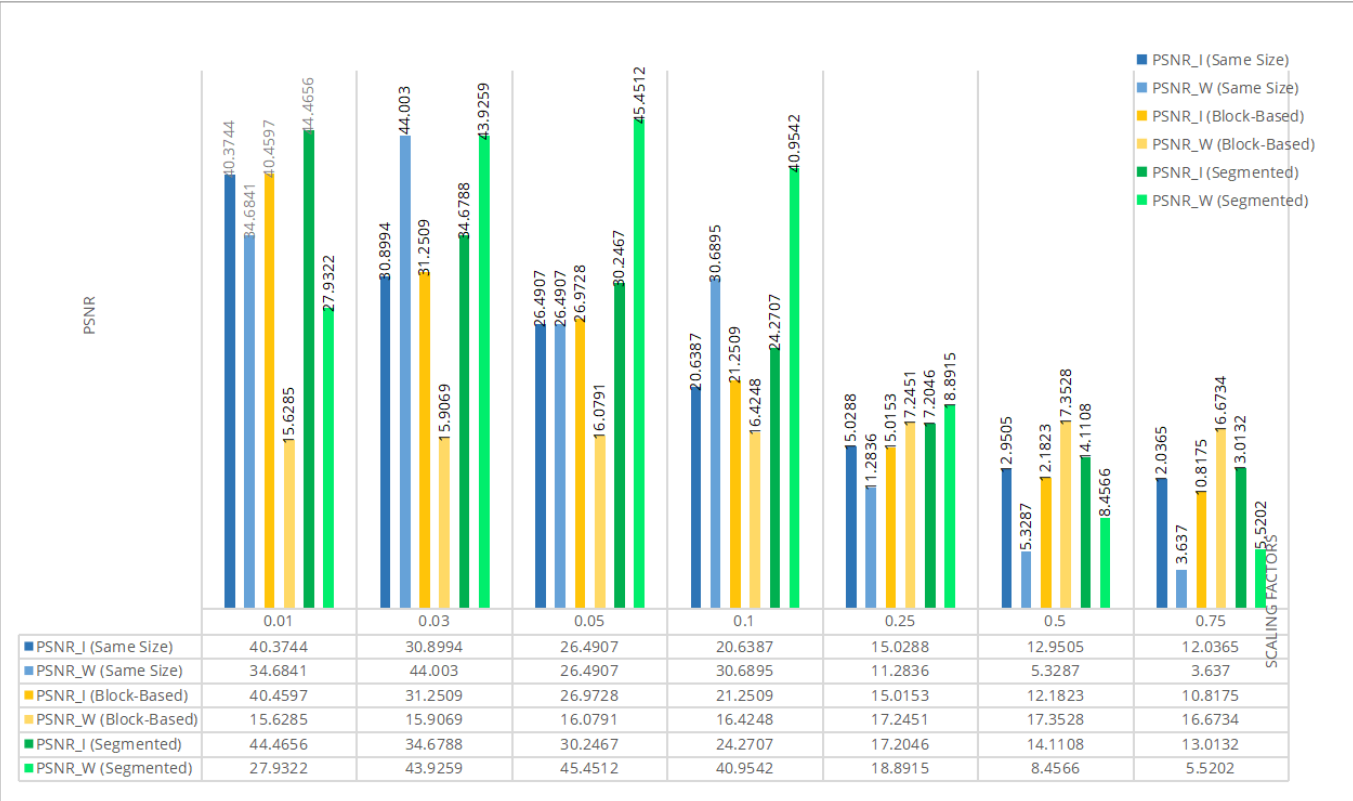


Figure 7. PSNR variation according to scaling factors for I1.

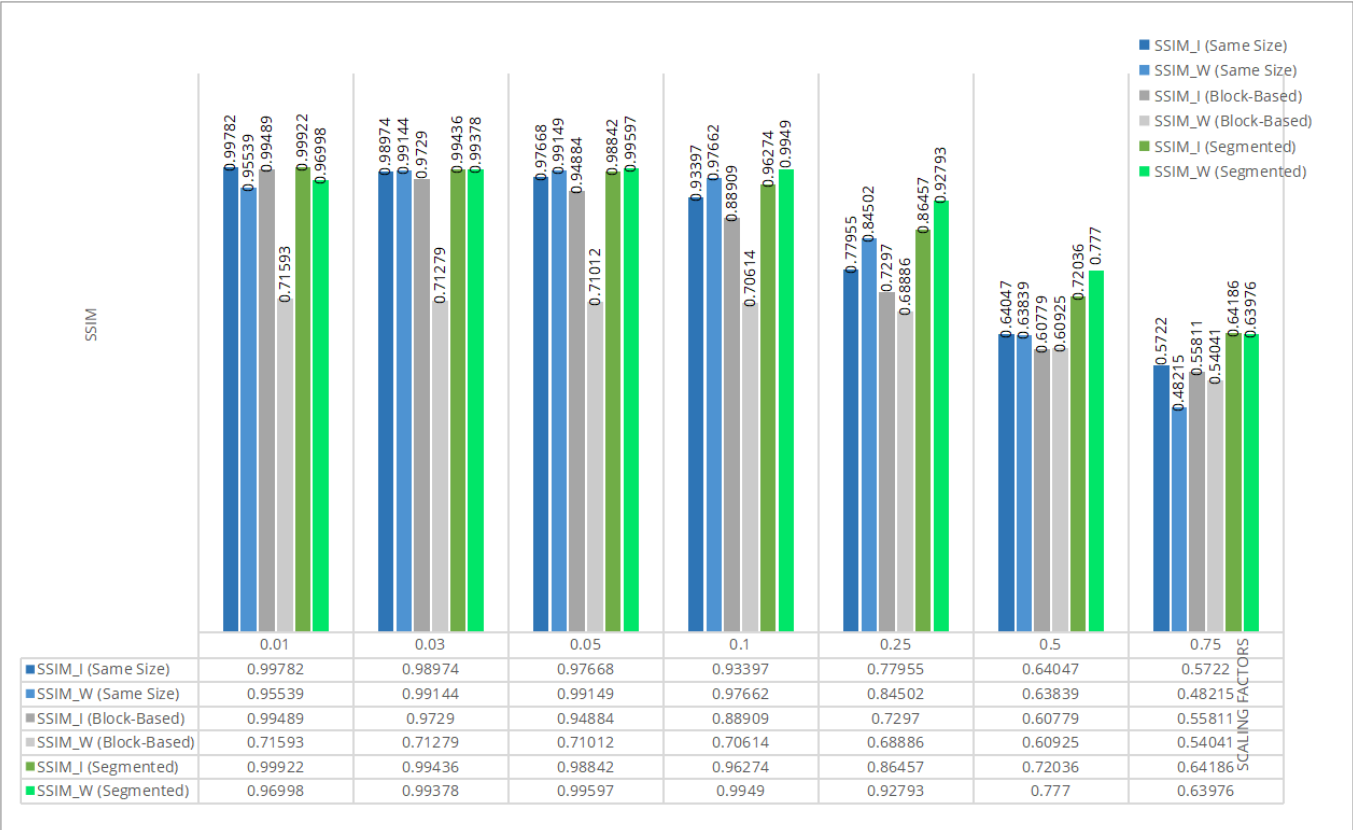


Figure 8. SSIM variation according to scaling factors for I1.

in this analysis. The evaluations were carried out on watermarked medical images obtained with a scaling factor of 0.01. Following the rotation attack, partial degradation in watermark quality was observed.

While a decrease was noted in metrics such as PSNR and SSIM, NC values also declined. This indicates that the rotation operation negatively affects the structural integrity of the watermark. When salt-and-pepper noise was added, a significant quality loss occurred in both the host image and the watermark. The notable drop in PSNR and SSIM values clearly reveals that the noise disrupts the visual similarity of the watermark. Similarly, low NC values indicate that the similarity between the extracted watermark and the original one is reduced. In the JPEG compression attack, the effects on the watermark were also prominent. The decrease in SSIM and NC values suggests that structural losses occurred after compression. Particularly in the W2 watermark, quality loss became more evident. The sharpening attack proved to be one of the most destructive. Significant drops were observed in all quality metrics as a result of this attack. While PSNR values decreased considerably, SSIM and NC values also suffered substantial reductions. This demonstrates that sharpening severely degrades both the structural integrity and perceptibility of the watermark.

Overall, it was observed that the proposed method demonstrates a certain level of robustness against attacks with a low scaling factor, but decreases in quality metrics were inevitable. Increasing the scaling factor could enhance watermark robustness; however, it was not preferred in this study as it would cause distortion in medical images. Since the primary objective of the study is to preserve the integrity of medical images, a scaling factor of 0.01 offers the ideal balance. This factor ensures acceptable watermark extraction success with minimal distortion. The hybrid DCT-SVD-based invisible watermarking techniques developed in this study offer significant potential, particularly for protecting information privacy in medical images. However, to further enhance the performance of these methods, certain improvements and advanced applications are needed.

In particular, in the Second Method, the block selection strategy has a direct impact on performance. Therefore, smarter block selection algorithms can be developed to improve the results. In this context, block selection techniques guided by mathematical modeling or based on statistical features may be applied.

Furthermore, the integration of artificial intelligence-based optimization algorithms can enable the automation of watermark placement. Techniques such as genetic algorithms, particle swarm

optimization (PSO), or artificial neural networks can be used to optimize the placement region and size of the watermark, resulting in more efficient outcomes in terms of both robustness and confidentiality. Indeed, in a study conducted by [22] using the Moth-Flame Optimization algorithm, the effectiveness of optimization-based approaches in the image segmentation process was demonstrated; this may serve as a guiding framework for the integration of similar optimization techniques into invisible watermarking processes.

For future studies, it is recommended to explore not only DCT-SVD but also methods involving different transform domains. In particular, alternative frequency-based hybrid approaches such as SVD-based DWT (DWT-SVD) or SVD-based DFT (DFT-SVD) could lead to the development of more robust and attack-resistant watermarking techniques. Such techniques can offer higher protection in terms of both security and data integrity in medical imaging.

Data Availability Statement

Data will be made available on request.

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Conflicts of Interest

The authors declare no conflicts of interest.

AI Use Statement

The authors declare that no generative AI was used in the preparation of this manuscript.

Ethical Approval and Consent to Participate

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